

# 1 DWT based Identification of Amyotrophic Lateral Sclerosis using 2 Surface EMG Signal

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## 6 **Abstract**

7 In the process of identification of Amyotrophic Lateral Sclerosis (ALS) which is a motor  
8 neuron disorder, extraction of feature is the most important step. In this work normal and  
9 ALS class for identification and monitoring have been included. Analysis of surface  
10 electromyography (sEMG) signal for ALS identification using discrete wavelet transform is  
11 most simple and powerful method being used all over the world. Time domain parameters,  
12 like Zero Crossing Rate (ZCR) and Root Mean Square (RMS) and frequency domain  
13 parameters like Mean Frequency (MF) and Waveform Length (WL) are considered. Threshold  
14 values for the above mentioned parameters are calculated for both the normal and ALS  
15 classes. Discrete Wavelet Transform (DWT) parameters are considered and their threshold  
16 values are also calculated for both normal and ALS classes. Surface EMG (sEMG) signal  
17 database of normal and ALS patients for both male and female is considered.

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19 **Index terms**— ALS, sEMG, ZCR, RMS, MF, WL, DWT.

## 20 **1 I. Introduction**

21 uman body is made up of large number of different bundles of muscle fibers. These all bundles of fibers are  
22 arranged functionally into different motor unit which are activated by nerve impulse which is very minute electrical  
23 pulse provided by the brain's nervous systems. These electrical impulses travel through the whole length of muscle  
24 fiber spread throughout in the body. Hence very small electric currents are generated by these bundles of muscle  
25 fibers during muscle force production [1]. The electromyography (EMG) signal is an electrical responses generated  
26 by the nerve cells of the brain in the form of electrical pulses from the contraction and relaxation of bundles  
27 of muscles throughout the body. sEMG is an electrical signals associated with the uppermost layer of muscles  
28 which are the electrical impulses generated and controlled by motor nerve unit of brain [2]. sEMG consists of the  
29 information in the form of electrical impulses about the various muscle activities in the body. Obtaining SEMG  
30 signals are of two different types [3]. First method of recording sEMG is with a surface electrodes and second  
31 method is insertion needle electrode which is called as intra electrode. By applying conductive solution to the  
32 skin surface and placing the electrodes on it, sEMG recording is done. It contains important information

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36 India. e-mails: sschorage@gmail.com, sschorage@gmail.com about the activity of muscles, status of its health,  
37 and its characteristics. There are two types of EMG signals are 1) Surface EMG (sEMG) 2) Intramuscular EMG  
38 (iEMG) [1]. In sEMG collection of muscle contraction or expansion information from the uppermost layer of  
39 muscle .Whereas in the case of iEMG collection of information is done from the deep inside the muscles in the  
40 body. To extract information from surface EMG signal, there are different methods of different time domain,  
41 frequency domain and time-frequency domain methods have been used. EMG is very important to diagnose  
42 many nervous disorders [1]. ALS is one among those Motor Nerve Disorder (MND).ALS, which is a progressive

### 4 III. METHODOLOGIES A) DISCRETE WAVELET TRANSFORM

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43 neurodegenerative disorder that affects the muscular activities of the body because of changes in the muscle  
44 configuration [1]. The EMG represents electrical activities inside the body. As EMG signal plays very important  
45 role as diagnostic tool for the MND patients, hence extracting important information from it is very important  
46 and having vast scope in its analysis process. To classify different MND diseases, feature extraction of SEMG  
47 is very important. Here one of those feature extraction techniques are presented based on wavelet transforms [1]  
48 [3]. The rest of the paper has been arranged as, in the next section which is section II, the related work is stated.  
49 Section III explains the methodology of the identification using feature extraction. The section IV explains about  
50 the results obtained in the process and its analysis which is in the terms of discussion. In the last section V  
51 conclusion is stated.

## 52 3 II. Related Work

53 Work proposed by Shaikh Anowarul Fattah et.al [1], is based on feature extraction of EMG using discrete  
54 wavelet transform. The time domain and frequency domain features have been discussed along with discrete  
55 wavelet transform features. The time domain feature discussed in this paper is zero crossing rate and the  
56 frequency domain feature discussed is mean frequency. Wavelet transform coefficients are explained in detail.  
57 Wavelet transform used is three level decomposition coiflet transform. Accuracy of the time and frequency domain  
58 feature extraction methods are compared with wavelet transformation method.

59 Work done by A. B. M. Sayeed Ud Doulah et.al [2], EMG signal is studies and examined in short time fourier  
60 transform for the detection of the ALS disease. Shapes and firing rates of motor nerve unit are the important  
61 features analyzed for the detection of neuromuscular disease. For the same study, timefrequency domain method  
62 has been considered. Use of spectrum analysis for the extraction of features has been done. The Short Time  
63 Fourier Transform method for the classification of EMG signals to detect the ALS patients and distinguish normal  
64 group.

65 Work done by Amol Lolure and V. R. Thool [3], is on the extraction of features from EMG and it has been  
66 evaluated in scatter graph. Extraction techniques have been applied for the recognition of hand movements.  
67 Scatter graphs which are actually mathematical diagram tool for evaluating the performance of EMG features.  
68 Mean absolute value is the key parameter has been considered which has been obtained from coefficients has  
69 shown the better performance in EMG signal analysis for hand and finger movement recognition.

70 Work done by Hossein Parsaei et.al [4], is the decomposition of EMG signal using the supervised technique of  
71 feature extraction. Signal decomposition techniques are discussed. Fisher discriminant analysis and supervised  
72 principal component analysis have been explored. The work proposed by the author is most beneficial in the  
73 decomposition of more complex signals. This work is quite useful for the decomposition of biomedical complex  
74 signals such as EMG in order to extract important information from them in order to detect the particular disease  
75 using the threshold values of the features.

76 Work done by P. Pal et.al [5], is the feature extraction for the detection of muscular atrophy. Knowledge-based  
77 expert system design and disease diagnosis is explored for the classification of EMG signal which is very hard  
78 to classify because of non stationary nature of the signal. Here on-line and off-line classification of EMG signal  
79 focusing mainly on disease diagnosis based on muscular atrophy approach.

## 80 4 III. Methodologies a) Discrete Wavelet Transform

81 Wavelet transform has been proved to be very powerful mathematical tool for biomedical signal processing as  
82 it can process non stationary time varying complex signals. Wavelet transform techniques are of two types.  
83 1) Discrete wavelet transformation (DWT) 2) Continuous wavelet transformation (CWT). In this paper DWT  
84 has been chosen because the application is in real time engineering signal application and the biomedical signal  
85 involved here is in complex nature. In discrete wavelet transform method, it iteratively transforms interested  
86 real time signals into multi-resolution two domain subsets of coefficients of wavelet transform which contains the  
87 information about the non stationary signal which can be used to analyze the complicated signal. Coiflet wavelet  
88 transform has been used for the decomposition of EMG signal in order to detect the neuromuscular disorder  
89 ALS.4level decomposition of wavelet transform has been used. Hence 5wavelet transform coefficients are used as  
90 characteristic parameters.4level decomposition means signal undergoes low pass and high pass filtering 4 times  
91 to give 4 low pass filter coefficients and 1 coefficient from last stage high pass filter. b) Different Features 1) Root  
92 Mean Square (RMS): Time domain parameter considered is RMS which is one of the well known features in time  
93 domain for analysis of the EMG. It is defined as the square root of the arithmetic mean of the squares of a set  
94 of values. It shows the power contain in the signal. It is the most common mathematical tool for defining the  
95 effective voltage and current of a non stationary signal. Mathematically it is represented as,????? = ?[ 1 ?? ?  
96 ?? ?? 2 ]  
97 ?? ??=1  
98 (1)

99 2) Waveform length (WL): WL describes the complexity of non stationary EMG signal. It is defined as the  
100 cumulative length of the EMG waveform over the particular focused time period segment N where n is the number  
101 of signal samples being considered. Mathematically it is expressed as,?? ?? = ? |?? ??+1 ? ?? ?? | ?? ??=1(2)

102 3) Mean Frequency (MF): It is defined as a pitch measure which shows the center of the distribution of power  
 103 across the all frequencies in the spectrum. It represents the smooth estimation of the concentration of spectral  
 104 power contain. It is a summation of all the frequencies under consideration divided by total frequencies present  
 105 over the particular time segment. Mathematically it is expressed,  $\text{MF} = \frac{\sum f_i \cdot \text{power}_i}{\sum \text{power}_i}$  (3)

## 106 5 IV. Results and Discussions

107 EMG database of 30 normal male and 15 normal females of age between 22 to 35 and 40 to 67 having normal  
 108 body shape is been considered. For ALS patients also 30 male and 15 female EMG database is been considered.  
 109 The features on the basis of which detection of ALS and classifying them into two group of normal class and ALS  
 110 class are considered as follow. Mean frequency which is the frequency domain feature showing the comparison  
 111 between normal and ALS class. Here the bubbled line shows the graph for normal person and plain line shows  
 112 the graph for ALS patient. Following graph shows the MF in normal person is more stable as compares to  
 113 ALS person. MF is more for ALS patient than normal. But this frequency domain parameter does not give us  
 114 accuracy in every case. Hence for more accurate results we are exploring the other techniques. Another frequency  
 115 domain feature we considered is waveform length which is denoted as WL and which refers the complexity of  
 116 the waveform in the particular time segment. Following graph shows the graph of WL for both normal and ALS  
 117 person. WL is more in ALS than that of normal persons. Another time domain parameter we considered here  
 118 is Zero crossing rate for both the class. ZCR is greater in ALS than that of in normal persons. Following graph  
 119 shows the comparison for ZCR between normal and ALS patients.

## 120 6 V. Conclusion

121 To identify the ALS disease on the basis of feature extraction from the sEMG database we have used the 4level  
 122 decomposition wavelet transform to get the multi-dimensional resolution of higher accuracy than the conventional  
 123 time and frequency domain analysis.

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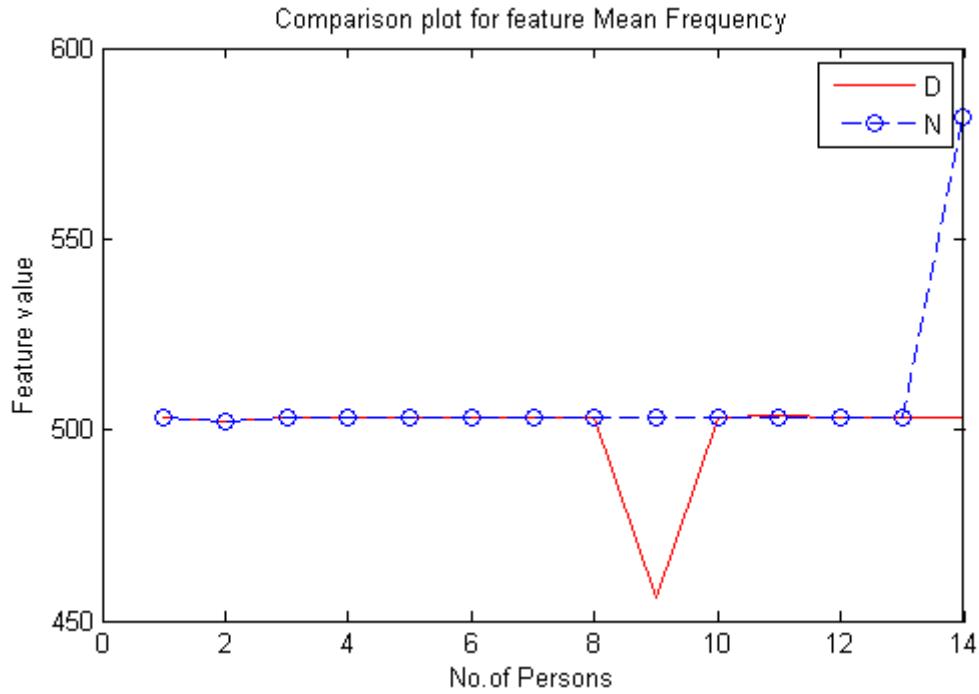


Figure 1: Fig. No. 1 :

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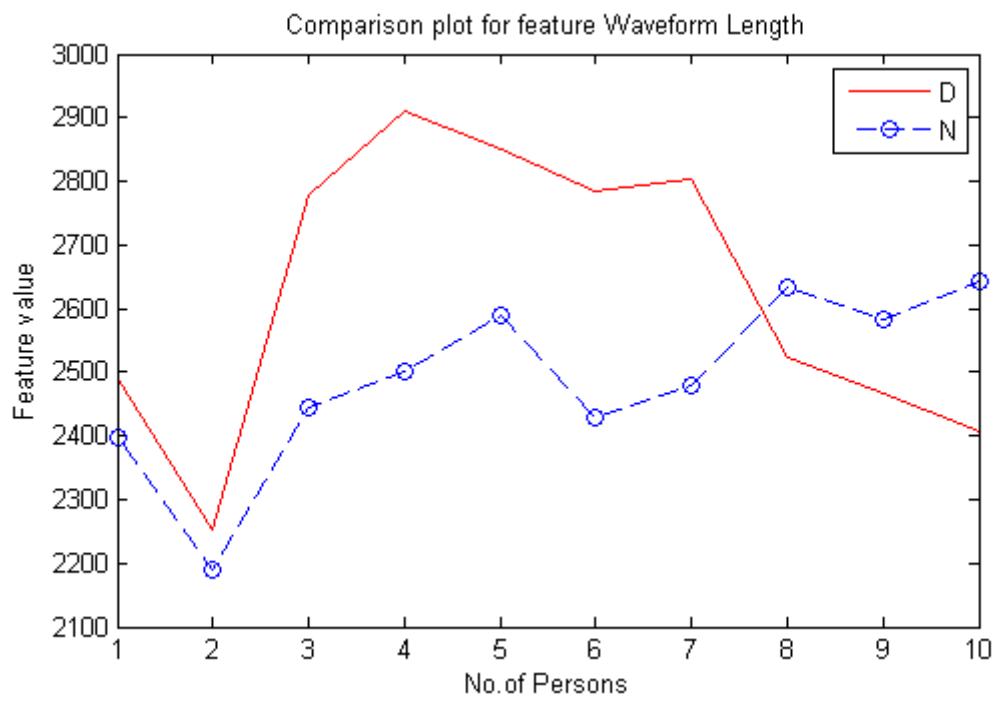


Figure 2: Fig. No. 2 :

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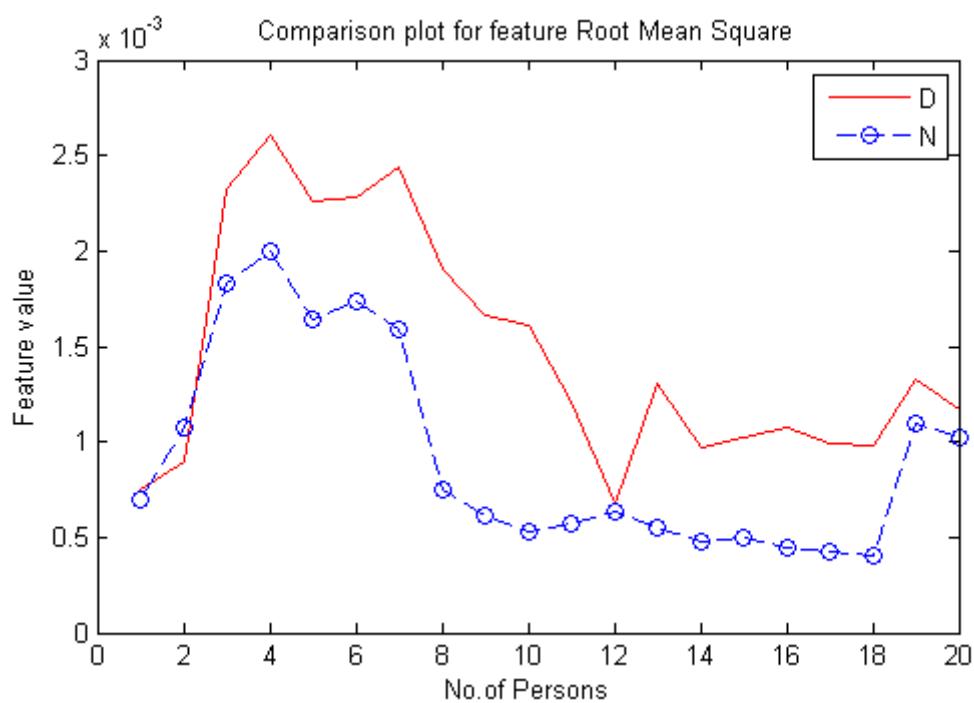
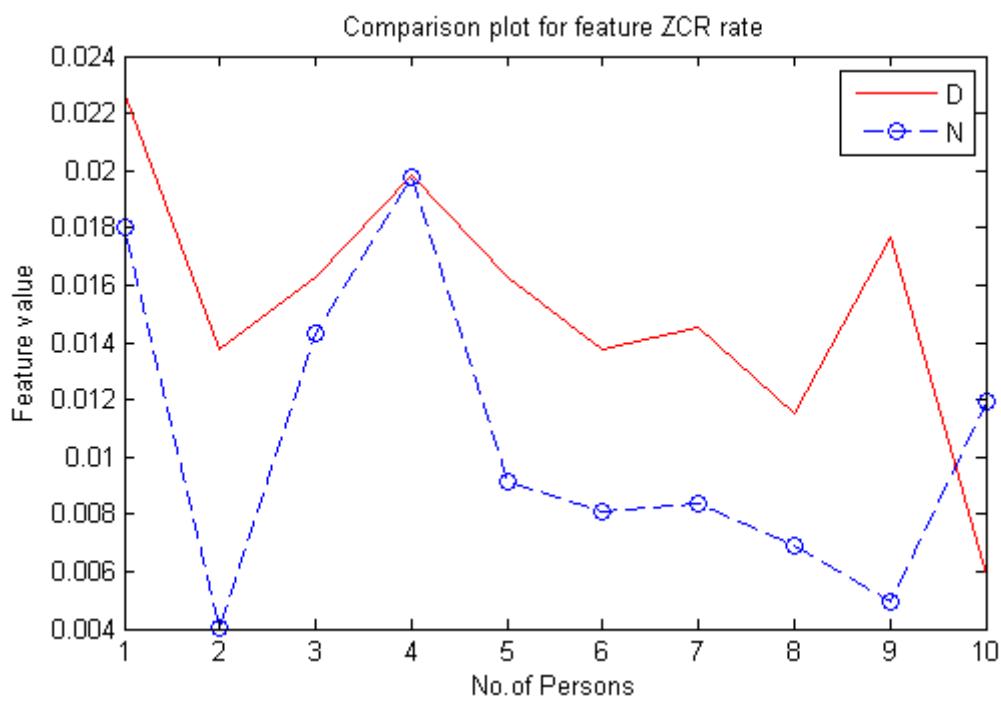


Figure 3: Fig. No. 3 :



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Figure 4: Fig. No. 4 :

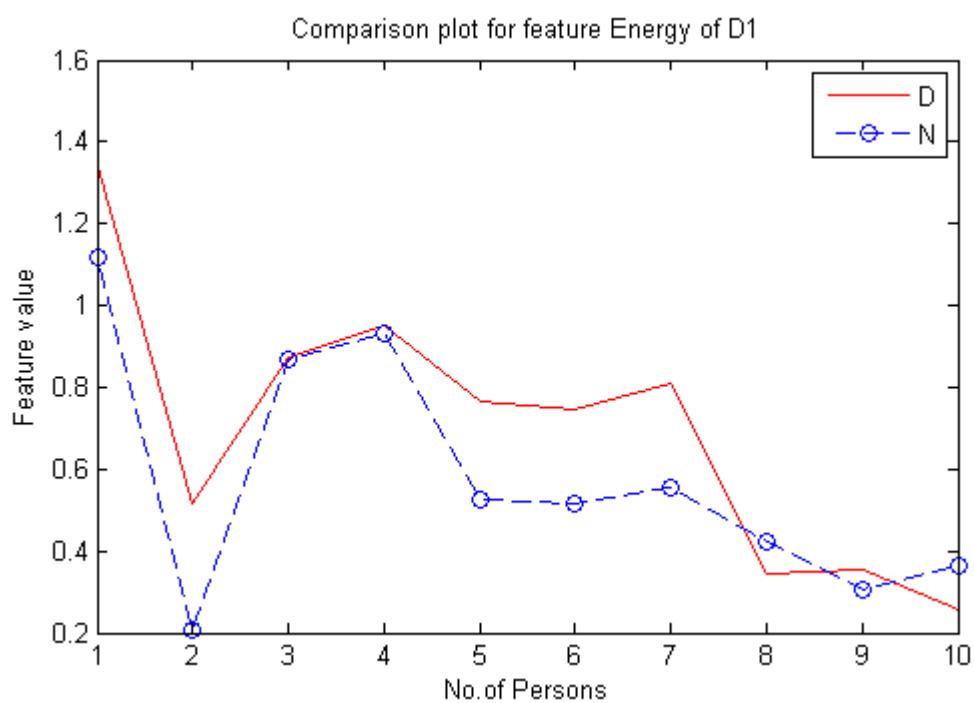


Figure 5: F

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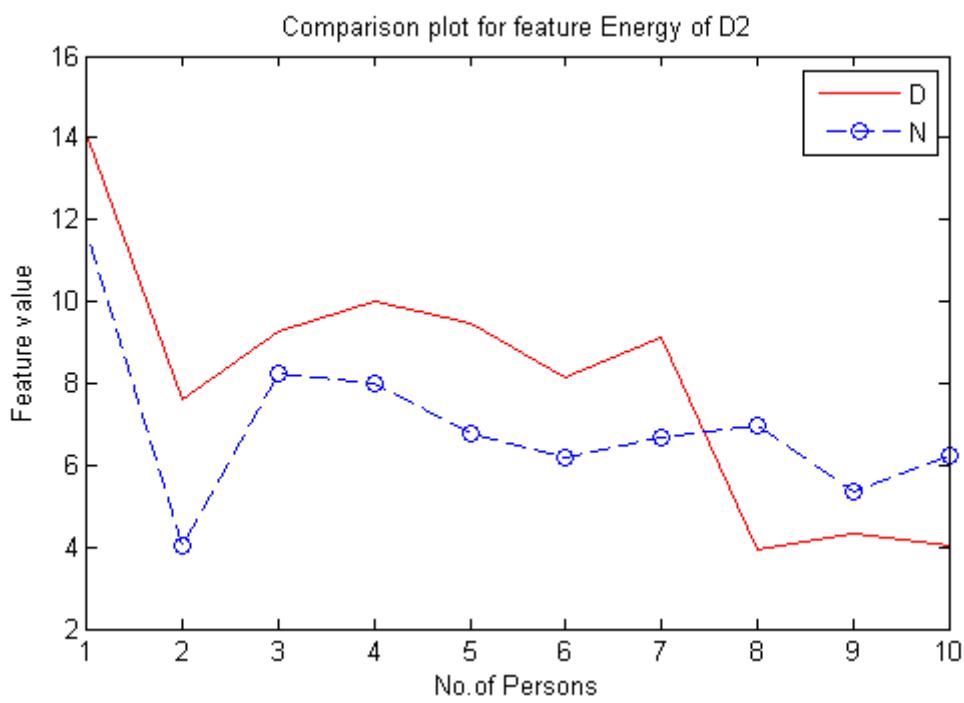


Figure 6: Fig. No. 5 :

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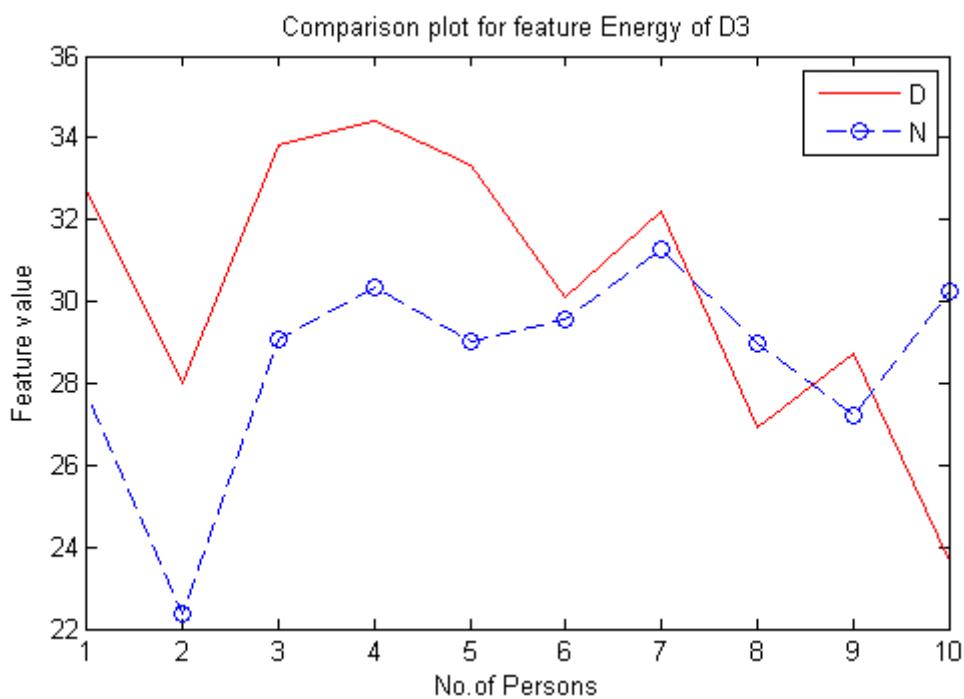
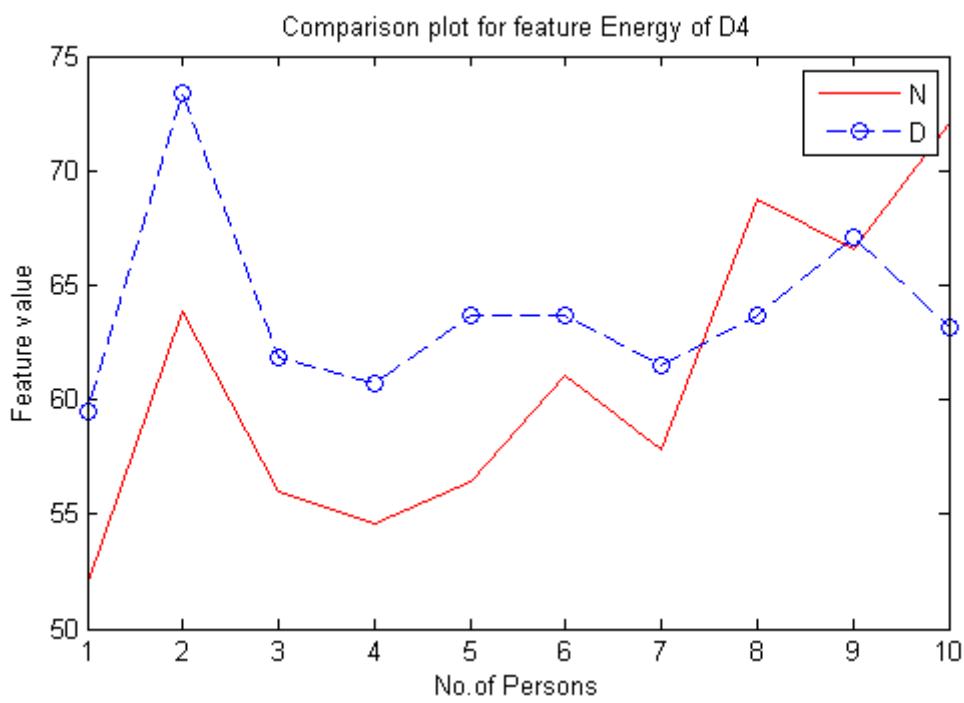
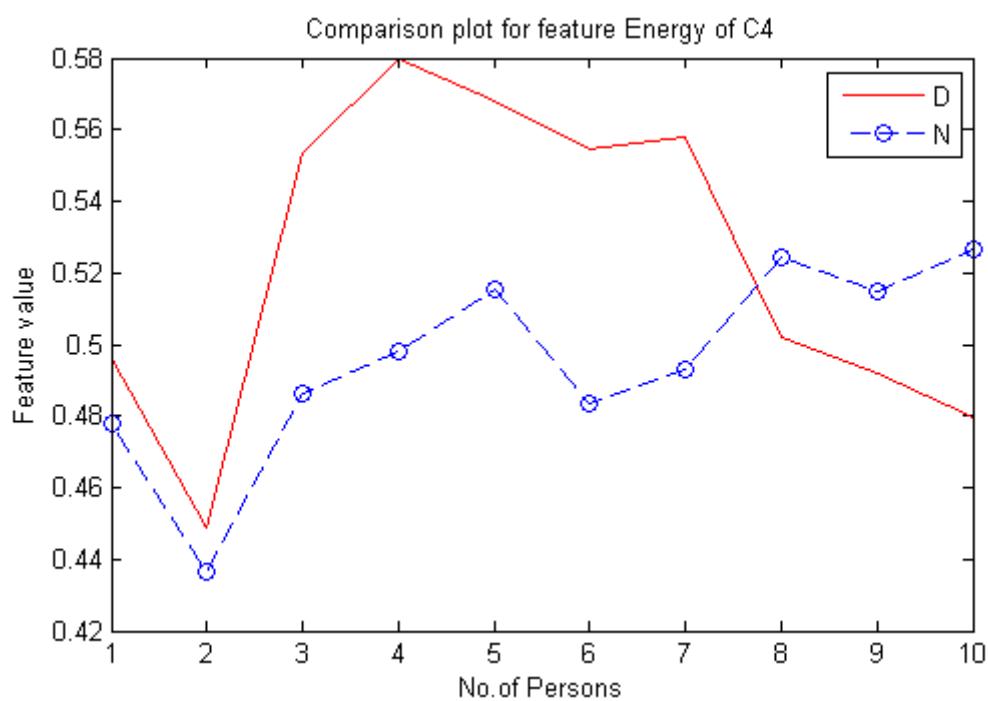


Figure 7: Fig. No. 6 :



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Figure 8: Fig. No. 7 :



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Figure 9: Fig. No. 8 :

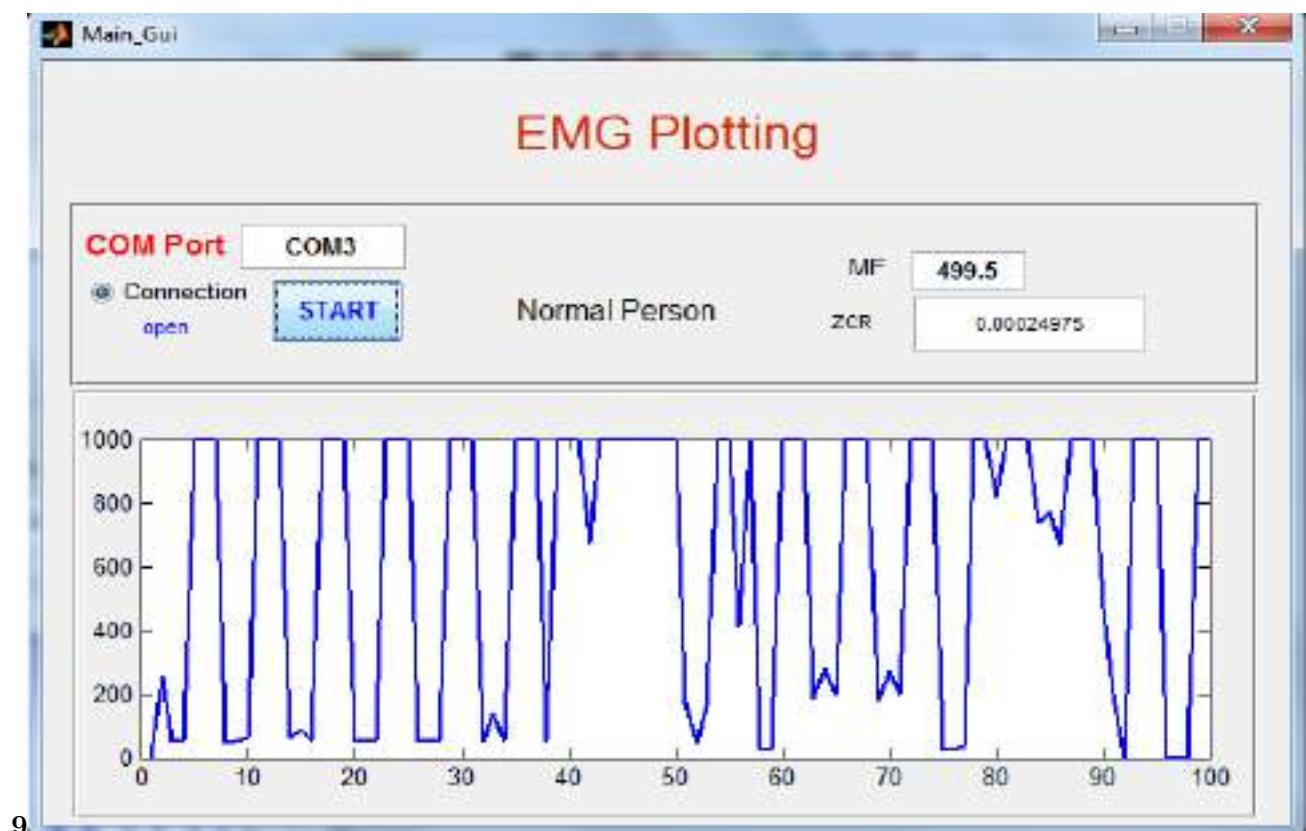


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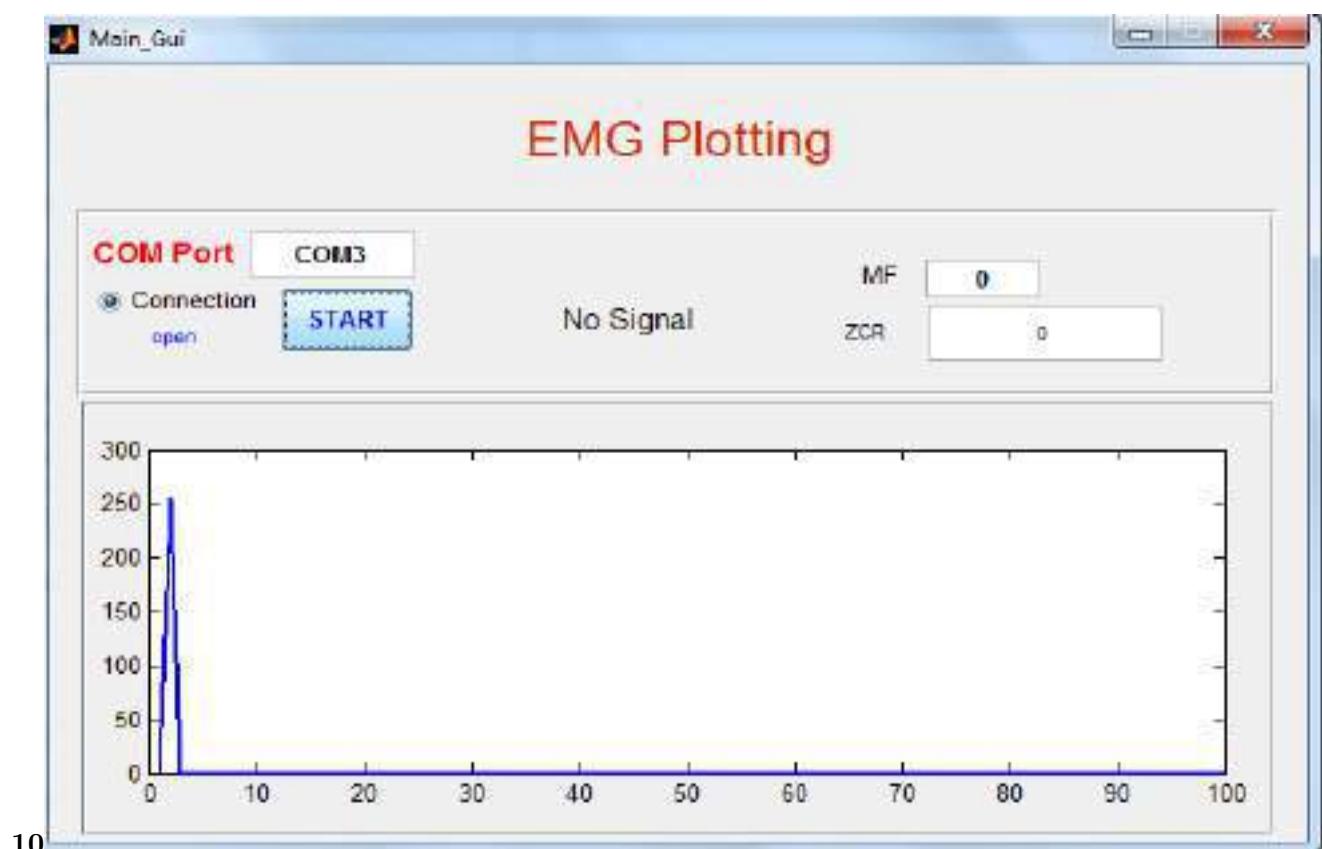


Figure 11: Fig. No. 10 :FF

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## No1

Sr. No.	Parameter Name	Threshold in normal	Values	Threshold Values in ALS
1.	Mean Frequency	502		503
2.	Waveform Length	2535		2750
3.	Root Mean Square	1.525		2.575
4.	Zero Crossing Rate	0.010		0.0114
5.	Energy of D1	0.5125		0.875
6.	Energy of D2	7.120		9.70
7.	Energy of D3	30.5		31.6
8.	Energy of D4	59.9		63.2
9.	Energy of C4	0.496		0.483

Figure 12: Table No . 1 :



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