Artificial Intelligence formulated this projection for compatibility purposes from the original article published at Global Journals. However, this technology is currently in beta. Therefore, kindly ignore odd layouts, missed formulae, text, tables, or figures.

Proniosomal Gel: Formulation and Charecterization of an 1 Antifungal Drug (Butenafine Hcl) Loaded Proniosomes for 2 **Topical Delivery** 3 Thimmaraju D \mathbb{R}^1 and Dr. Abdul Nasir Kurnool² Δ ¹ Adichunchanagiri College of Pharmacy 5 Received: 9 December 2019 Accepted: 1 January 2020 Published: 15 January 2020 6

Abstract 8

The present proniosomal gel investigation was aimed to minimize the adverse effects 9

associated with present topical butenafine hydrochloride formulations and made to enhance its 10

bioavailability and sustained release by novel proniosomal drug delivery system. Butenafine 11

hydrochloride is an allylamine class of advanced antifungal drug. Which mainly recommended 12

to treat long term topical fungal infection. Proniosomes were prepared by slurry method using 13

different concentrations of non-ionic surfactant (span and tween) and evaluated various 14

parameter like surface morphology, entrapment efficiency, drug content, viscosity, drug 15

content, in-vitro 16

17

Index terms— butenafine hydrochloride, fungal infection, proniosomes, slurry method, in-vitro diffusion 18 studies, antifungal activity 19

1 Introduction 20

he main target of drug therapy is to provide therapeutic amount of drug concentration to proper site in the body 21 to produce desired therapeutic efficacy. Now a days in the field of pharmaceutical industries are put great efforts 22 towards the prefabrications of existing drugs and their delivery systems, to break the problem related to poor 23 24 solubility, Author ?: Department of Pharmaceutics, Sri Adichunchanagiri College of Pharmacy, Adichunchanagiri 25 University, B.G Nagara, Mandya-571448, Karnataka, India. e-mail: rajustyle28595@gmail.com stability, toxicity, bioavailability, dosage problem etc. 1 Topical administration is a preferable route for direct, local therapy, in that 26 it is Non-invasive and is directly applied to the invading site and reduces systemic adverse effects. However, it is 27 not possible to use all types of drugs (antifungal drugs) through transdermalroute. 2 The drawbacks of topical 28 antifungal formulation such as cream, lotions, spray etc. may include difficult to apply in deep dermatophytic 29 infections, inadequate amount leads poor response, inability to apply difficult to reach area such as natal cleft, 30 low effectiveness, redness of skin, stinging and burning sensations as side effects. 3 Various attempts have been 31 made to improve the skin permeation of drugs like use of permeation enhancers, electroporation, microneedles, 32 needleless injection, thermophoresis, etc. But these methods damaging the protective barrier function of the skin 33 and may cause irritation or other skin problems. 4 Hence, to overcome the problems associated with topical 34 35 antifungals formulations, this study is intended to formulate novel drug delivery system such as Proniosomal 36 gel for topical administration with model anti-fungal drug, in order to enhance skin permeation as well as to 37 sustain the drug release for prolonged period of time. 5 There are many novel drug delivery systemshave been investigated by pharmaceutical scientists to fulfil these criteria and considerations for topical delivery of drugs. In 38 that nanocarrierssuch as Proniosomescan make their way easily to hair follicles and they may show accumulation 39 between corneocytes, skin having high lipid content so it can easily combining with lipidic layer, Proniosomes 40 also have the capability to control/sustain the drug release, which reduces the side effects and dosing frequency 41 of drugs. ? Proniosomes reduces the physical stability problems of niosomes such as fusion, aggregation, leaking 42 43

on storage.

6 PREPARATION OF BUTENAFINE HYDROCHLORIDE PRONIOSOMAL GEL

? It also controls hydrolysis of encapsulated drugs which limiting the shelf life of the dispersion.

? The entrapment of both hydrophilic and hydrophobic drugs can be done easily by this vesicular system. 8
? Sustained and controlled release of drugs can be done due to depot formation.

47 ? More stable and Ease of use. ? It leads to ease the transportation, better size distribution and storage
 48 uniformity of dose.

? These formulations are biodegradable, biocompatible and non-immunogenic to the body. 9 Butenafine 49 hydrochloride is a synthetic benzylamine antifungal agent. It is indicated for the topical treatment of the following 50 dermatologic infections: Interdigital Tinea pedis (athlete's foot), Tinea corporis (ringworm) and Tinea cruris 51 (jock itch) due to E. floccosum, Tinea mentagrophytes, T. rubrum, and T. tonsurans, tinea (pityriasis) versicolor 52 due to M. furfur. 10 Butenafine Hcl is a synthetic antifungal agent that is structurally and pharmacologically 53 related to allylamine antifungals. The exact mechanism of action has not been established, but it is suggested 54 that butenafine's antifungal activity is exerted through the alteration of cellular membranes, which results in 55 increased membrane permeability, and growth inhibition. Butenafine is mainly active against dermatophytes 56 and has superior fungicidal activity against this group of fungi when compared to that of terbinafine, naftifine, 57 tolnaftate, clotrimazole, and bifonazole. It is also active against Candida albicans and this activity is superior to 58 59 that of terbinafine and naftifine. Butenafine also generates low MICs for Cryptococcus neoformans and Aspergillus 60 fumigatus as well. 11 The aim of the current study was to develop a topical formulation which would be effective 61 against transdermal fungal infection as well as overcome the drawbacks of current topical/ oral therapy. The 62 butenafine hcl loaded proniosomal gel formulation is prepared by slurry method with some modifications. The formulations are evaluated for its vesicle size, entrapment efficiency (EE), viscosity, spreadability, skin permeation, 63 and stability. 64

65 2 II.

⁶⁶ 3 Materials and Methods

Materials and sources: Butenafine hydrochloride were supplied as a gift sample by Glenmark Pharmaceuticals
 Ltd. Mumbai. Cholesterol and soya lecithin were purchased Yarrow chem products, Mumbai, India. Span-60,

⁶⁹ Tween-60 were purchased from SD fine Chem. Ltd. Mumbai, India, Chloroform and Ethanol Merck Specialties⁷⁰ PVT. LTD. All other chemicals and reagents used were of analytical grade and were used without further

71 purification.

$_{72}$ 4 Methods:

Characterization of drug and other excipients: Characterisation was done by Fourier transfer infrared spectroscopy (FT-IR) (Make: Brukers alpha t-series, Software: Opus) of butenafine hydrochloride and other was performed. The drug and excipients were kept in 1:1 ratio at 5°C in refrigerator to observe any reaction which may take place between drug and excipients. The mixtures of samples were analysed by FT-IR after one month

⁷⁷ along with standard drug and excipients as the reference.

78 5 Procedure for preparation of proniosomes

The current proniosomes were prepared by adopting slurry method using maltodextrin as carrier. The 79 composition of different proniosome formulation were prepared by using various non-ionic surfactants and 80 cholesterol in different molar ratios and drug is represented in Table-01. The solvent such as chloroform and 81 ethanol (2:1) were used to dissolve ingredients. The physical mixtures and solvent were mixed thoroughly in the 82 beaker using sonicator/glass rod. Then, an accurately weighed amount of maltodextrin was added slowly to above 83 resultant solution with continuous stirring to obtain slurry, otherwise it forms clump mass because maltodextrin 84 was water soluble. Additional quantity of solvent was added to form slurry, in case of lower surfactant loading. The 85 obtained solution was immediately transferred to round bottomed flask and attached to rotary flask evaporator 86 to evaporate solvents at temperature $45\pm 2^{\circ}$ C, 60-70 RPM and reduced pressure 600-700mm of Hg respectively. 87 After complete removal of solvent from the flask, thin layer of proniosomes was obtained. Then, further dried 88 overnight in a desiccator (containing cacl 2 / silica) under vacuum at room temperature to get dry, free-flowing 89 proniosomal powder. The obtained proniosomes was stored in a tightly closed container at 4°C until further 90 evaluation. The composition of different proniosomal formulations were represented in Table -01. 91

Proniosomes were transformed into niosomes by hydrating using phosphate buffer (pH 6.8), the niosomes were sonicated twice for 2 min. using a sonicator. These niosomes were used in the formulations of gels. 12

⁹⁴ 6 Preparation of butenafine hydrochloride proniosomal gel

Butenafine hydrochloride proniosomal gel was prepared by using 1% w/w of Carbopol-940 as a gel base. Carbopol-940 was soaked overnight in 100ml distilled water then mixed with niosomal suspension and required quantity of 97 preservatives (methyl/ propyl paraben) were added.Triethanolamine was added drop wise to the formulation for 98 an adjustment of required skin (pH5.8-6.0) and also to obtain gel at required consistency. The prepared butenafine 99 hcl. proniosomal gel was stored in the refrigerator until further evaluation studies. 13 The photomicrography 100 was carried out using optical microscope. A dry Proniosomes were hydrated using saline buffer pH 6.8, then drop of suspension were mounted on glass slide and observed under the microscope with magnification of 40X for morphological observation. The photomicrograph of the preparation obtained from the optical microscope by using a digital SLR camera.

¹⁰⁴ 7 ii. Morphology study by Scanning electronic microscopy ¹⁰⁵ (SEM)

The sample of proniosomes is placed in an evacuated chamber and scanned in a controlled manner by an electronic 106 beam. The dried proniosomes were mounted on to stubs by using double-sided adhesive carbon tape. Then 107 proniosomes were analyzed after gold sputtering to yield a gold film of 30 nm thickness. In the SEM (Joel, JSM-108 5600LV, japan), interaction between electronic beam and vesicles produces a variation in the physical phenomenon 109 that can be obtained in the form of images. These obtained images used for surface characteristics. 14 iii. Particle 110 size analysis Particle size analysis was carried out using optical microscope. The optical microscope was fitted 111 with a stage micrometer to calibrate the eyepiece micrometer. A dry Proniosomes were hydrated usings a line 112 buffer pH6.8 or NaCl then drop of suspension were transferred onto a clean glass slide and observed under the 113 microscope. Before placing the cover slip sample was dispersed uniformly with the help of a brush, size of 100 114 niosomes from the batch were measured in terms of eyepiece division. 15 115

¹¹⁶ 8 b) % Entrapment efficiency

To determine the % EE, 20mg of Proniosomes were taken in beaker and was dissolved in 20ml of cosolvents of Ethanol and buffer pH 5.8. The free butenafine hydrochloride was separated from proniosomes by ultracentrifugation (Eppendorf centrifuge 5430 R) at a speed of 14000 RPM for 30-45 min. at 4 0 C. after centrifugation 1ml of supernatant was taken and observed at 223nm using UV spectrophotometer (shimadzu-1800), to determine the amount of free drug in the formulations. 16

¹²² 9 c) Viscosity and pH studies

Viscosity of the prepared proniosomal gel is evaluated by using Brookfield viscometer (model-DV2TRVTJ0) with spindle No. RV-07(7) at 100 rpm. 100 g of the proniosomal gel was taken in a beaker and the spindle was dipped in it. The viscosity of gel was measured at temperature of 25°C. The readings of 03 were taken for average ofsamples then calculate the viscosity.

The pH of each formulation was measured using a calibrated digital pH meter. The readings were taken for average of 3 samples. The normal range of topical gel pH is 5.5-8 respectively. 17

129 10 d) Spreadability

For the determination of spreadability, excess of sample was applied between the two glass slides and was compressed to uniform thickness by placing 1000 gm weight for 5 min. Weight (50 gm) was added to the pan. The time required separating the two slides, i.e. the time in which the upper glass slide moves over the lower plate was taken as measure of spreadability (S). The standard range of gel spreadability is 8.4-15gm.cm/sec. respectively. 18 Spreadability (g.cm/s) (S) = $M \times L/T$ Where M = weight tied to upper slide, L = length moved on the glass slide, T= time taken.

¹³⁶ 11 e) In-vitro drug release studies i. Method for egg membrane ¹³⁷ preparation

The contents of egg shells were removed and then it was dipped in the dilute hydrochloric acid (0.1N) for 30 min. The egg membrane was separated manually and washed thoroughly with distilled water. 19 ii. Drug release studies

In vitro release studies were carried out using Franz diffusion cells with a receptor compartment volume 141 of 20 mL and an effective diffusion area of 3.14 cm 2 . Egg membrane was used as diffusion membrane. A 142 predetermined amount of gel containing proniosomes was placed on the donor compartment and 20ml of freshly 143 prepared phosphate buffer of pH 5.8 is placed in receptor compartment. The receptor medium was continuously 144 stirred using magnetic stirrer at $37\pm0.5^{\circ}$ C. At predetermined time intervals, 0.1 mL samples were withdrawn 145 from the receiver compartment and replaced with an equal volume of fresh buffer. The collected samples were 146 analyzed at 223 nm by using UV spectrophotometer. 20 f) In-vitro antifungal studies 9.75gm of Potato dextrose 147 148 agar was taken in a 250 mL conical flask and dissolved in 250 mL of distilled water. The medium was sterilized 149 in an autoclave at 15 lbs for 30 min. After sterilization, the medium was kept aside at room temperature. Then 150 medium was poured into sterilized Petri dishes to get 3-4 mm depth uniformly in front of laminar airflow unit. After solidification, a loop of diluted suspension culture (Candida albicans) in nutrient broth was added on to 151 the surface of solidified agar and was spread homogeneously with the help of L shape rod. After stabilization of 152 culture, Gels of known concentration along with pure drug were fed into the petridish with the help of sterile 153 disk. Then Petri dishes were incubated for 48 h at 37 °C. After incubation the zone of inhibition was measured. 154 21155

¹⁵⁶ 12 g) Stability studies of the most satisfactory formulation

Optimized formulations of butenafine loaded proniosomal gel were subjected to accelerated stability testing as 157 per ICH guidelines for short term and placed in a screw capped glass container and stored at ambient humidity 158 conditions and temperatures 40°C (75 \pm 5RH) for a period of 30 days. The samples were analyzed for physical 159 appearance, pH, drug content, and in vitro drug release at regular interval of 30 days. 22 IV. Particle size has 160 increased with increase in concentration of polymer, with constant drug load and concentration of other agents. 161 However, size was reduced with increase in concentration of surfactant and mean size of particles depends upon 162 on the rotational and temperature of the rotavapor. The results of particle size of each formulations were found 163 to be 33.85-40.03?m and tabulated in table no. 02. 164

165 **13** Result and Discussion

$_{166}$ 14 b) % Entrapment efficiency

Entrapment efficiency was found to increase with increase in polymer (cholesterol) Concentration. Increase in size 167 of proniosomes with increase in concentration of polymer and drug has resulted in increase in drug entrapment 168 efficiency and also improves the stability of the bilayer membrane of the vesicles. Cholesterol decreases leakage 169 of drug molecule from bilayer vesicle structure and also provides spherical smooth surface to the bilayer vesicles. 170 Entrapment efficiency of proniosomes formulations ranged from 64.41% to 79.87%. niosomes formed from 171 span 60 proniosomal gel exhibits higher EE than other surfactant formulations (i.e. span 40, tween 60). Span 172 60 is solid at room temperature and have highest phase transition. Span 60 is having the same head group with 173 different alkyl chains and might lower the HLB value and thus increases the EE of the drug. Formulation F3 174 containing span 60: cholesterol in 1:2 ratio showed highest EE (79.87%) and tabulated in table no. 02. 175

¹⁷⁶ 15 c) pH and Viscosity

The pH values exhibited by gels are tabulated in table no. 03 and found in range of 5.40 to 6.11 at 25 0 C which is physiologically acceptable range for topical preparations.

The viscosity of the proniosomal gels were found in range 8920-14400 at 25 0 C, as concentration of Carbopol used in all the formulations is same (1%). The results of viscosity of each formulation were tabulated in table no. 03. when using spindle no. 07 respectively.

¹⁸² 16 d) Spreadability studies

Spread ability of the different proniosomal gel formulations were determined and tabulated in table no. 03. The spread ability range of gel were found to be 16.40-22.19 gm.cm/sec.

¹⁸⁵ 17 e) In-vitro drug release studies of the proniosomal gel

The release studies were carried out for all the butenafine hcl loaded formulations. The formulation which 186 shows the percentage of drug release maximum at 30 hrs. was considered as optimum. The percentage drug 187 release of all prepared formulation is compared with optimized formulation (F3 The release data was fitted to 188 various mathematical models to evaluate the kinetics and mechanism of drug release. The kinetic data of all 189 formulations F1-F9 could be best expressed by first order equation as the plots showed highest linearity (R 2 190 :0.340-0.395), then zero order release kinetics (R 2 :0.977-0.997). The release data of the optimal batch showed 191 F3 value of 0.997 and 0.395 for the zero order and first order respectively. The formulations were observed to 192 yield correlations with Higuchi model i.e. R = 2 = 0.994 thus indicating the diffusion mechanism. The 'n' values 193 obtained Korsmeyer-peppas model of F-3 was 0.443 which indicates that drug release swelling and mechanism 194 of release was Anomalous (non-Fickian) diffusion. The in-vitro antifungal activity of formulation was studied 195 by cup plate method. Results of the in-vitro antifungal activity are shown in table-06. The zone of inhibition 196 is more observed in butenafine hcl loaded proniosomal gel formulation (F3) compared to other formulation and 197 pure drug was taken as a standard. The marketed product (Butop-1% cream) showed less zone of inhibition 198 compared to optimized proniosomal gel formulation (F3). From the experimental outcome, it was concluded 199 that prepared proniosomes gel formulation exhibited promising antifungal activity. The stability studies of the 200 formulation were carried out according to ICH guidelines. The optimized formulations i.e. (F3) were subjected 201 to stability studies @ $40^{\circ}C$ (75 \pm 5RH) for a period of 30 days. The physical stability was assessed by the pH, 202 drug content, and % invitro drug release. The stability studies showed that there were no significant changes 203 in the abovementioned response variables. Thus, it can be concluded that the drug was found to be stable on 204 storage. 205

206 18 Conclusion

Result of the present study indicates that prepared butenafine loaded proniosomes gel formulation is an alternative route for transdermal drug deliveryto treat fungal infection. Proniosomes were prepared by slurry method using different concentration of cholesterol, surfactants, and soya lecithin etc. The prepared proniosomes were evaluated for % entrapment efficiency, spreadability, viscosity and % drug content. The values obtained were found to be

satisfactory and complies with standard range. The in-vitro drug release was found to increase with increase 211 in cholesterol (polymer) concentration and decreased with increase in surfactant concentration. In that F3 212 formulation exhibited highest drug release (75.46%) compared to other formulations over a period of 30 hours. 213 The in-vitro antifungal activity study was concluded that proniosomal gel formulation with drug (F3) shows 214 better zone of inhibition than the other formulations and marketed product. Stability studies demonstrated 215 there was no significant variation in pH, drug content and % in-vitro drug release and found to be stable at 216 the end of storage period (30days). From the above experimental data, it can be concluded that the transdermal 217 delivery of butenafine Hcl loaded proniosomal gel formulations can be used in the future for treatment of fungal 218 1 2 3 infection with improved bioavailability.



Figure 1: 6



Figure 2:

219

¹Proniosomal Gel: Formulation and Charecterization of an Antifungal Drug (Butenafine Hcl) Loaded Proniosomes for Topical Delivery

 $^{^{2}}$ © 2020 Global Journals

³Proniosomal Gel: Formulation and Charecterization an Antifungal Drug (Butenafine Hcl) Loaded Proniosomes for Topical Delivery



Figure 3: Figure 1 :



Figure 4: Figure 2 :



Figure 5: Figure 3 : Figure 4 :



Figure 6: Figure 5 :



Figure 7: Figure 6 :



Figure 8: Figure 7 :





Figure 9: Figure 9 : Figure 10 : Figure 11 :



Figure 10: Figure 12 :

1

Excipients

		Drug Bute- nafine	Soya lecithin	Maltod	extrin	*Surfa	ctants (mg)	*Cholester
Formulation code		Hcl (mg)	(mg)	(mg)				(mg)
		(0)			Span	Span	tween6	
					40	60	0	
	$\mathbf{PF1}$	20	100	500	100	-	-	100
	$\mathrm{PF2}$	20	100	500	200	-	-	100
	$\mathbf{PF3}$	20	100	500	100	-	-	200
	PF4	20	100	500	-	100	-	100
	$\mathbf{PF5}$	20	100	500	-	200	-	100
	$\mathbf{PF6}$	20	100	500	-	100	-	200
	$\mathbf{PF7}$	20	100	500	-	-	100	100
	$\mathbf{PF8}$	20	100	500	-	-	200	100
	$\mathbf{PF9}$	20	100	500	-	-	100	200
*Surfactant: cholester	ol-(1:1), (2:1),	(1:2) ratios	respectivel	у.				
Solvents: -Chloroform	: Ethanol (2:1)-PF1-PF9						
III.	Evaluatio	on Studies of						

Evaluation Studies of

Proniosomal Gel

[Note: B a) Characterization of Proniosomes i. Photomicrography]

Figure 11: Table 1 :

$\mathbf{2}$

SL.	FORMU	LAMELANN PARTICLE	% ENTRAPMENT
NO.		SIZE (µm)	EFFICIENCY
1	F1	35.69 ± 1.56	69.01 ± 2.71
2	F2	34.15 ± 1.45	71.34 ± 1.21
3	F3	40.03 ± 0.14	79.87 ± 1.93
4	F4	36.60 ± 1.81	64.41 ± 3.10
5	F5	34.74 ± 2.11	70.53 ± 1.58
6	F6	38.81 ± 0.56	72.32 ± 2.17
7	F7	33.85 ± 1.54	73.87 ± 3.89
8	F8	35.15 ± 2.21	65.37 ± 0.98
9	F9	37.80 ± 2.92	77.64 ± 1.89

Figure 12: Table 2 :

18 CONCLUSION

3

FORMU	L MEQN pH	VISCOSITY (CPS)	SPREADABILITY
			(gm.cm/sec)
F1	$5.69 {\pm} 0.04$	$8,920{\pm}0.02$	17.40
F2	$5.55 {\pm} 0.02$	$9,960{\pm}0.01$	21.27
F3	$5.97 {\pm} 0.02$	$13,960{\pm}0.03$	16.76
F4	$5.84{\pm}0.04$	$10,920{\pm}0.01$	18.80
F5	$5.40 {\pm} 0.03$	$11,\!680{\pm}0.04$	22.19
F6	$5.47 {\pm} 0.02$	$12,360{\pm}0.03$	17.25
F7	$6.11 {\pm} 0.01$	$9,800{\pm}0.05$	21.26
F8	$6.00 {\pm} 0.02$	$13,360{\pm}0.02$	19.03
F9	$5.93 {\pm} 0.01$	$14,400{\pm}0.01$	16.40

Figure 13: Table 3 :

 $\mathbf{4}$

). The prepare	d
----------------	---

Figure 14: Table 4 :

$\mathbf{5}$

Formulat	ti Ze ro order ki-	First order ki-	Higuchi's	Korr'speppas	n value
	netic	netics	model	Model	
F1	0.991	0.373	0.989	0.916	0.416
F2	0.989	0.382	0.986	0.929	0.412
F3	0.997	0.395	0.994	0.985	0.443
F4	0.985	0.377	0.991	0.929	0.426
F5	0.983	0.371	0.987		0.404
F6	0.994	0.366	0.991	0.983	0.422
F7	0.945	0.369	0.990	0.920	0.397
F8	0.977	0.340	0.981	0.918	0.401
F9	0.995	0.393	0.993	0.984	0.441

Figure 15: Table 5 :

SL.NO.	FORMULATION	ZONE OF (mm)	INHIBITION
1	Pure drug	18 ± 0.04	
2	Marketed product (butop-1%)	12	
3	F1	-	
4	F2	3	
5	F3	16	
6	F4	8.5	
7	F5	-	
8	F6	9.5	
9	F7	-	
10	F8	7.6	
11	F9	14.5	

Figure 16: Table 6 :

7

Sampling		Storage condition	
Interval		40 0 C ± 20 C /75% RH $\pm 5\%$ RH	
(days)	$_{\rm pH}$	Drug content	% in-vitro Drug re-
			lease
0	$5.97{\pm}0.02$	$99.13 {\pm} 2.13$	$75.46 {\pm} 0.62$
30	$5.93{\pm}0.01$	98.91 ± 1.12	$74.78 {\pm} 0.91$
V.			

Figure 17: Table 7 :

6

18 CONCLUSION

- [Balch and Cooke ()] 'A study of the composition of hen's egg-shell membranes'. D A Balch , R A Cooke .
 InAnnales de Biologie Animale Biochimie Biophysique 1970. EDP Sciences. 10 p. .
- [Gupta (2002)] 'Butenafine: an update of its use in superficial mycoses'. A K Gupta . Skin Therapy Lett 2002
 Sep. 7 (7) p. .
- [Desai et al. ()] 'Development and evaluation of antifungal topical niosomal gel formulation'. S Desai , A Doke ,
 J Disouza , R Athawale . Int J Pharm Pharm Sci 2011. 3 (5) p. .
- [Desai et al. ()] 'Development and evaluation of antifungal topical niosomal gel formulation'. S Desai , A Doke ,
 J Disouza , R Athawale . Int J Pharm Pharm Sci 2011. 3 (5) p. .
- [Kumar and Rai (2011)] 'Development and evaluation of proniosomes as a promising drug carrier to improve
 transdermal drug delivery'. K Kumar , A K Rai . International Research Journal of Pharmacy 2011 Nov. 2
 (11) p. .
- [Salve ()] 'Development and evaluation of topical drug delivery system for terbinafine hydrochloride using
 niosomes'. P S Salve . Research Journal of Topical and Cosmetic Sciences 2011. 2 (2) p. .
- [Shilakari Asthana et al. ()] 'Etodolac containing topical niosomal gel: formulation development and evaluation'.
 G Shilakari Asthana , A Asthana , D Singh , P K Sharma . Journal of drug delivery 2016. 2016.
- [Rao and Kamble (2018)] 'Formulation and evaluation of antifungal proniosomal gel for oral candidiasis'. M Rao
 P Kamble . Journal of Drug Delivery and Therapeutics 2018 Jul 14. 8 (4) p. .
- [Bomma et al. (2017)] 'Formulation Development and Evaluation of Proniosomal Powder of Candesartan'. G
 Bomma , S M Harika , A M Babu , V Bakshi . Analytical Chemistry Letters 2017 Jul 4. 7 (4) p. .
- 239 [Gurrapu et al. (2012)] Improved oral delivery of valsartan from maltodextrin based proniosome powders.
- Advanced Powder Technology, A Gurrapu, R Jukanti, S R Bobbala, S Kanuganti, J B Jeevana. 2012 Sep
 1. 23 p. .
- [Kumar and Rajeshwarrao (2011)] Nonionic surfactant vesicular systems for effective drug delivery-an overview.
 Acta pharmaceuticasinica B, G P Kumar, P Rajeshwarrao. 2011 Dec 1. 1 p. .
- [El-Laithy et al. (2011)] 'Novel sugar esters proniosomes for transdermal delivery of vinpocetine: preclinical
 and clinical studies'. H M El-Laithy , O Shoukry , L G Mahran . European journal of pharmaceutics and
 biopharmaceutics 2011 Jan 1. 77 (1) p. .
- [Mathur et al. (2014)] 'Physical and chemical penetration enhancers in transdermal drug delivery system'. V
 Mathur , Y Satrawala , M S Rajput . Asian Journal of Pharmaceutics 2014 Aug 23. 4 (3) . (Free full text articles from Asian J Pharm)
- [Yoshioka et al. ()] 'Preparation and properties of vesicles (niosomes) of sorbitan monoesters (Span 20, 40, 60 and 80) and a sorbitantriester (Span 85)'. T Yoshioka, B Sternberg, A Florence. Int J Pharm 1994. 105 p. .
- 252 [Lam et al. (2018)] Recent advances on topical antimicrobials for skin and soft tissue infections and their safety
- concerns. Critical reviews in microbiology, P L Lam , K K Lee , R S Wong , G Y Cheng , Z X Bian , C H
 Chui , R Gambari . 2018 Jan 2. 44 p. .
- [Abdou and Ahmed ()] 'Terconazole proniosomal gels: effect of different formulation factors, physicochemical
 and microbiological evaluation'. E M Abdou , N M Ahmed . J Pharm Drug Deliv Res 2016. 5 (1) .
- [Abdou and Ahmed ()] 'Terconazole proniosomal gels: effect of different formulation factors, physicochemical
 and microbiological evaluation'. E M Abdou , N M Ahmed . J Pharm Drug Deliv Res 2016. 5 (1) .
- [Poojary (2017)] 'Topical antifungals: A review and their role in current management of dermatophytoses'. S A
 Poojary . Clinical Dermatology Review 2017 Oct 1. 1 (3) p. .
- [Poojary (2017)] 'Topical antifungals: A review and their role in current management of dermatophytoses'. S A
 Poojary . Clinical Dermatology Review 2017 Oct 1. 1 (3) p. 24.
- [Kaur and Kakkar (2010)] Topical delivery of antifungal agents, I P Kaur, S Kakkar. 2010 Nov 1. 7 p. . (Expert
 opinion on drug delivery)
- 265 [Verma and Utreja (2019)] 'Vesicular nanocarrier based treatment of skin fungal infections: Potential and
- emerging trends in nanoscale pharmacotherapy'. S Verma, P Utreja. Asian Journal of Pharmaceutical
 Sciences 2019 Mar 1. 14 (2) p. .